INVESTIGATING THE EFFECTS OF LAMOTRIGINE ON HCN CHANNELS: A TEST CASE FOR A NEW MINIATURIZED PATCH-CLAMP AMPLIFIER Alessandro Porro¹, Michele Rossi², Filippo Cona², Federico Thei², Anna Moroni¹, Bina Santoro³ ¹ Department of Biosciences, University of Milan, Italy ² Elements SRL, Cesena, Italy ³ Department of Neuroscience, Columbia University, New York, NY, USA

L3729-Pos

There are contrasting reports in the literature on the effects of lamotrigine (LTG), a widely used anticonvulsant drug, on modulation of native Ih currents in neurons. Poolos et al. [1] reported an increase in current mainly due to a positive shift in the activation curve of the channel, while Peng et al. [2] reported an increase in maximal current but no shift in the voltage dependency. To better understand these results we expressed the main components of the I_h current in neurons, HCN1 and HCN2, separately in HEK293T cells and measured their functional properties in the absence or presence of LTG. In addition, we assessed LTG effects obtained in the presence of the neuronal HCN channel auxiliary subunit TRIP8b [3]. Measurements were performed using a new all-in-one integrated amplifier prototype, designed and developed by Elements SRL, the ePatch. The miniaturized ePatch amplifier is USB plug-n-play and integrates the analog front-end with multiple gains stage, the analog-to-digital converter and filters all into a single small headstage without any external bulky case.



col is shown (right). Currents were recorded in whole cell configuration, at R.T., 24h after transfection of HEK293T cells with hHCN1 and mTRIP8b 1a4 (where indicated) cDNAs. B, Activation curves obtained from tail currents collected at -40mV. Fitting the Boltzmann equation to data yielded the following values of half activation voltage ($V_{1/2}$) and inverse slope factor (s). Top, HCN1 (black line), $V_{1/2}$ = -71.7 ± 1.2 mV, s = 7.8 ± 1.5 mV, N=4; HCN1 + 100 \mu M LTG (red line), $V_{1/2}$ = $-72.6 \pm 0.6 \text{ mV}$, s= 7.4 ± 0.5 mV, N=4. Bottom, HCN1 + TRIP8b (black dash line), $V_{1/2} = -80.9 \pm 0.4 \text{ mV}$, s= 7.7 ± 0.3 mV, N=5. C, Mean normalized tail current density. Top, HCN1 (black), 8.3 \pm 1.95 pA/pF, N=4 and HCN1 + 100 μ M LTG (red), 18.7 \pm 1.7 pA/pF, N=5. Data are presented as mean \pm SEM. All data were acquired at 5 kHz using ePatch amplifier.

Introduction

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The ePatch is controlled by the EDR3 EPISODIC software interface that enables an easy control of the amplifier and displays data in real time, both in the gap-free or episodic modalities. Input current ranges, bandwidth, voltage stimulus and electrode offset compensation can all be easily selected and modified. Moreover it has the following peculiarities:

- real-time data analysis (I/V graph for channel conductance and reversal potential, FFT, etc.)
- continuous membrane resistance and capacitance monitoring (R and C values can be automatically saved for every sweep)
- digital LabBook to manually record events and experimental details such as used cell line, buffer solutions, etc.
- data outputs saved in different formats: .dat (e.g. Matlab™), .abf (e.g. pClamp™)
- available for Windows and Mac OS

The results of our experiments show that lamotrigine does not have a direct effect on HCN channels, suggesting that the reported increases in I_h activity in neurons may result from indirect effects of the drug on other cellular components. This finding may also explain the contrasting results observed following lamotrigine application to native I_h currents in distinct neuronal types, and implies that lamotrigine may not necessarily act to increase I_h conductance in all cells and conditions. The recordings demonstrate the high-quality data acquired by the ePatch, which are comparable to those acquired by state-of-the-art amplifiers in terms of signal to noise ratio and data content.



We thank Nick Poolos for helpful comments and suggestions during the study. This work was supported by Fondazione CARIPLO grant 2014-0796 to A.M. and B.S





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ePatch details

- The miniaturized ePatch amplifier integrates in a small headstage the low-noise amplifier, the pulse generator and the digitizer into only 42 x 18 x 78 mm and it is connected directly to the USB port of a laptop without the need of any other external bulky digitizer. It has the following features:
 - Open input (RMS) noise: 150 fA rms @ 1kHz 480 fA rms @ 10 kHz 4 pA rms @ 100 kHz
 - Current ranges: ± 200 pA (Gain 2.25G Ω), ± 2 nA (Gain 225M Ω), ± 20 nA (Gain 22.5M Ω), ±200nA (Gain 2.25M Ω)
 - Max sampling rate: 200 kS/s
 - Parametric voltage protocols for pulse generator in the range of ± 500 mV
 - C-fast C-slow R-series P/N compensations
 - C fast compensation range: 0 11 pF
 - R series compensation range: 0 10 MΩ
 - Auto electrodes voltage offset fine compensation
 - Continuous C-membrane and R-seal estimation
 - Programmable digital I/O
 - Zap pulse
 - Digital filters: cut-off frequencies in the range between 62,5 Hz and 100 KHz USB powered
 - Dovetail or rod bar mounting
 - Compatible with standard pipette holders (BNC or SMA connectors)



Conclusions

References

[1] Poolos NP et al. (2002) Nat Neurosci. 5(8):767-74. [2] Peng BW et al. (2010) Neuropsychopharmacology. 35(2):464-72. [3] Santoro B et al. (2009) Neuron. 62(6):802-13